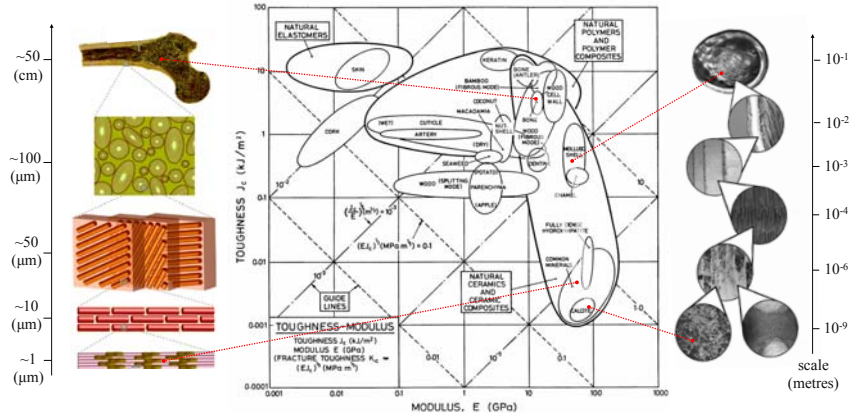
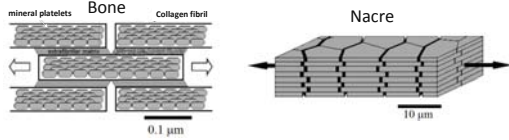


Main findings: 1) High fracture toughness of mineralized biological composites is explained by modeling.
2) The proposed model offers guidelines useful for novel designs of tough artificial composites.

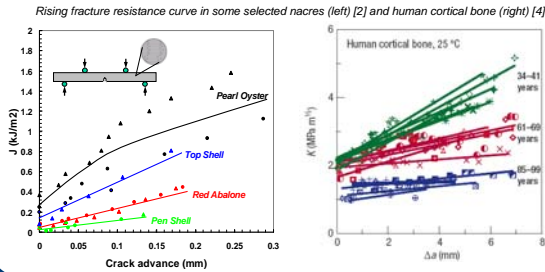
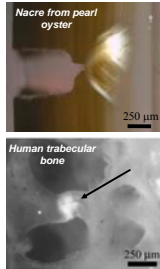
I. Introduction

- The "staggered structure" is found in hierarchical structure of several high performance biological composites such as bone and nacre.
- The staggered structure consists of stiff mineral inclusions aligned along one direction with some overlap, and bonded by softer proteins.
- This unique structure leads to interesting combinations of stiffness, hardness and toughness [1] yet it is largely underused in biomedical and bioengineering applications.
- Mechanics of biological composites needs to be elucidated. In particular, which mechanisms are behind their "toughness amplification"?



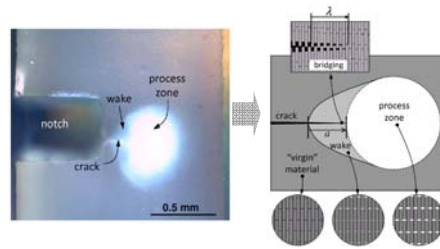
II. Fracture toughness: experiment

- Fracture toughness: the ability of material to resist crack propagation
- "Stress whitening" occurs in nacre and bone due to light scattering by the voids created by large deformations (images to the right) [2,3].
- Nacre and bone possess high fracture toughness.
- On top of being tough, nacre and bone exhibit a rising crack resistance curve making it harder for the crack to further propagate.
- Rising fracture toughness results in structural stability even though nacre and bone inherit natural flaws.



III. Fracture toughness: modeling

- Nacre is chosen as the representative of biological staggered structures for modeling.
- In nacre, tablet bridging and process zone are the two main toughening mechanisms.
- Stress whitening ahead of the crack tip represents the process zone.
- We developed an analytical model to predict fracture resistance curve, $\tilde{J}(\tilde{a})$.
- Fracture resistance is purely expressed in terms of the properties of the structure (i.e. material properties and structural parameters).



| Material properties | Structural parameters |
|-----------------------------------|------------------------------------|
| Tablet modulus E_m | Tablet thickness t |
| Interface shear modulus G_i | Tablet aspect ratio $\rho = L/t$ |
| Interface shear strength τ_s | Mineral content $\phi = t/(t+t_i)$ |
| Interface toughness J_i | |

Model

Composite properties

Elastic modulus E Failure strain ϵ_{max}

Tensile strength σ_s **Fracture toughness $\tilde{J}(\tilde{a})$**

$$\tilde{J} = \frac{2}{\pi} \tilde{a} \left(1 - \alpha F \left(\frac{d\tilde{J}}{d\tilde{a}} \right) \right) \quad \text{for } 0 \leq \tilde{a} \leq \frac{\pi}{2}$$

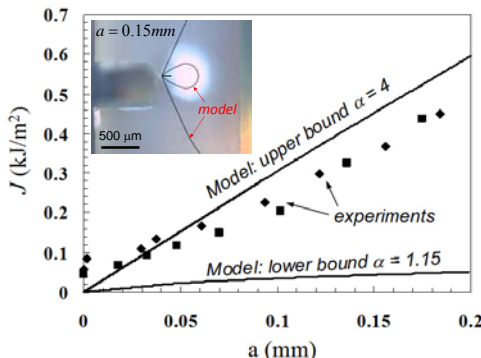
$$\tilde{J} = \frac{1}{1 - \alpha F \left(\frac{d\tilde{J}}{d\tilde{a}} \right)} \quad \text{for } \frac{\pi}{2} < \tilde{a}$$

$$\alpha = \frac{1}{4} \left(\frac{E \epsilon_{max}}{\sigma_s} - 1 \right)$$

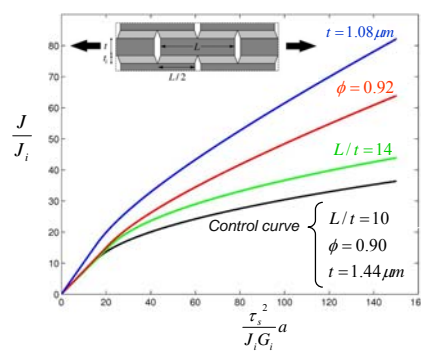
$$F(n) = 2 \left(\frac{(1+n)\sqrt{1+2n}}{n} - n \cot^{-1} \left(\frac{n}{\sqrt{1+2n}} \right) - \frac{(1+2n)^2}{n^2} \ln \left(\frac{1+2n}{1+n} \right) \right)$$

IV. Results

- The modeling results are in excellent agreement with experiments conducted on top shell [4].

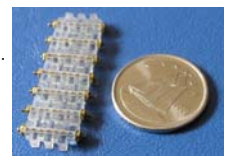


- Using small tablets with high aspect ratio and high volume concentration leads to high toughness [5].



V. Conclusions

- The analytical model proposed here can explain high fracture toughness of biological mineralized composites.
- Tablet bridging and process zone toughening largely contribute to the toughness of the staggered composite.
- This study provides implications for novel designs of artificial tough ceramics with biomedical and biomimetic applications.



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